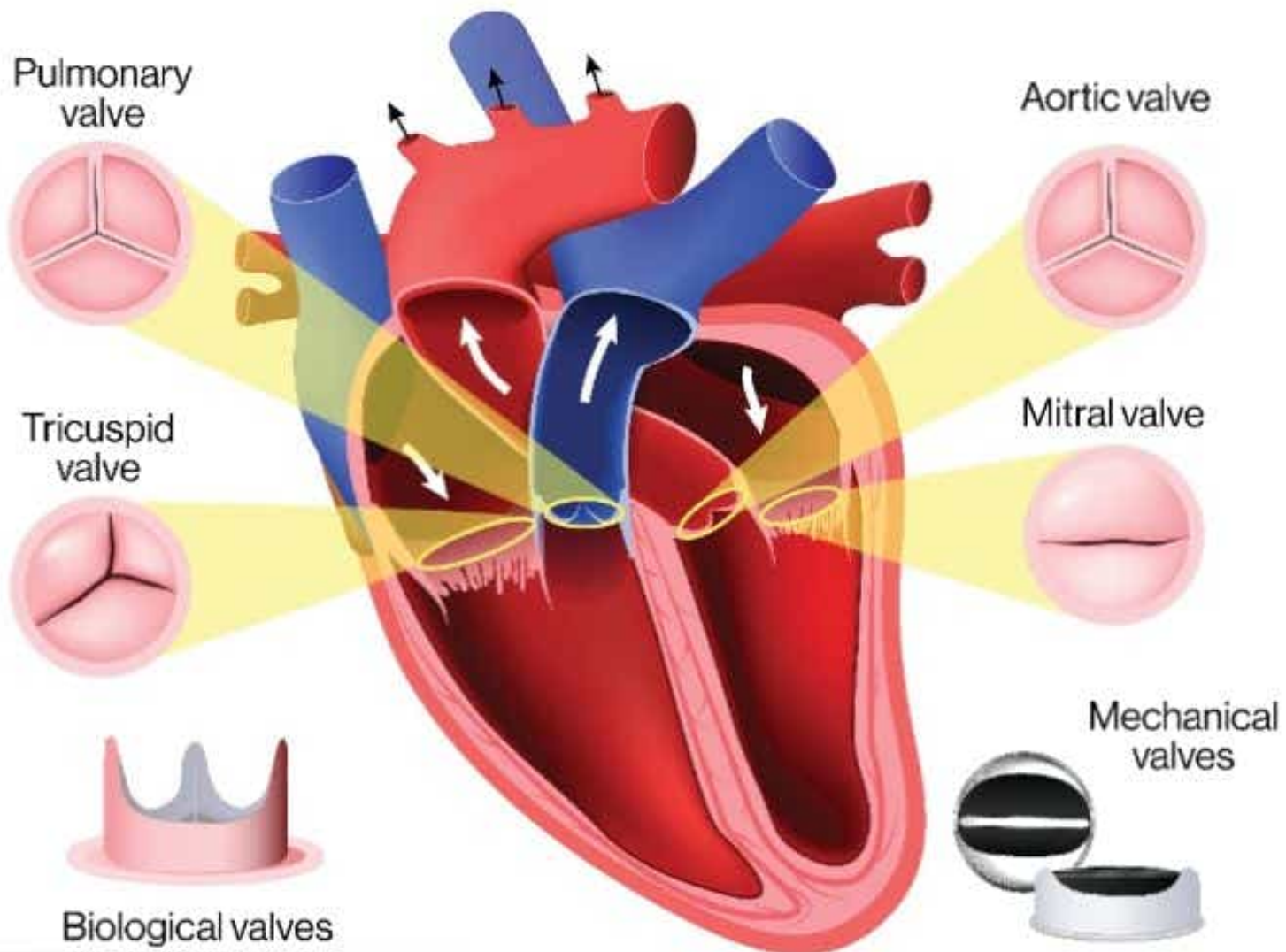


# Heart valve



electronics are worn externally. Without any major surgery and without any risk of infection this circuit can work for a long time. The transmitter part can be made at the cost of a dollar and hanged in the neck. A small receiving antenna and a passive detector (without battery) in the form of a pill (radio pill) can be surgically placed inside the heart with the stimulating electrode at the ventricular muscle.

Figure 5.13 shows the block diagram of a telemetry type RF energised pacemaker. A free running multivibrator generates the desired pulses at the rate of 70 beats/minute. The pulses are used to turn a R.F. oscillator of frequency 2 MHz. The pulses modulate the R.F. oscillations. The modulated R.F. waves are amplified and transmitted through a transmitter coil. The receiver coil receives these modulated R.F. waves. The capacitor and rectifier, connected to the receiver coil which is placed beneath the skin remove the 2 MHz carrier. Thus the output of the rectifier diode is used to stimulate the heart muscle. This type is also not liked by the cardiac patients.

#### 5.4 ARTIFICIAL HEART VALVES

Today cardiac surgery has advanced tremendously to enable repair of all congenital heart defects, replacement of damaged valves and bypassing of coronary blocks. About 1000 babies is born with deformed heart and 1/3 of them die in infancy. The improper functioning of the heart is due to various defects like hole in the heart, atrial septal defects and ventricular septal defects. In several cases like pulmonary stenosis, the valves of the major vessels are narrow. When the major vessels of the heart are wrongly connected, there is mixing of pure and impure blood. This accounts for the blue colour of the baby. These defects must be corrected as early as possible to save the life of the patient. For young people, the mitral valve and aortic valve can be affected. The tricuspid valve may be affected at a later stage. Badly diseased valve has to be replaced by an artificial valve. There are two types of valves:

- i) **Prosthetic valves:** These are made from high grade plastics and metal. They need a long coagulating agent (i.e.) blood thinning agent. The average durability of these valves is about 8 to 10 years.
- ii) **Tissue valves:** These may be either homograft or heterograft. Homograft valves are taken from human beings. Heterograft valves are taken from animals. Here blood thinning agent is not necessary. The average durability of these valves is smaller than the prosthetic valves. Only the prosthetic or mechanical valves are discussed here.

##### 5.4.1 Requirements for the design of artificial heart valves

- i) When the artificial heart valve is in contact with the blood, there would not be any hemolysis or blood clots.



- i) The valve material must be tough enough to withstand the heart beat rate throughout the life of the patient.
- ii) It should be designed small, light, reliable and efficient enough to enable it to be inserted surgically into the heart.

### Different natural heart valves

Since the left side of the heart is the one which normally functions with much higher pressure differentials, the left heart valves are usually failed to function properly. The **mitral valve** is located between the left atrium and the left ventricle and the **aortic valve** is located between the right ventricle and right atrium will fail. Occasionally the **tricuspid valve** which is located between the right ventricle and right atrium will fail. The procedure in valve replacement involves opening the chest (thoracotomy), placing the heart on bypass using a heart-lung machine, cutting through the heart muscle to expose the valve, excising the diseased valve and the surrounding tissue and attaching a prosthetic valve in its place.

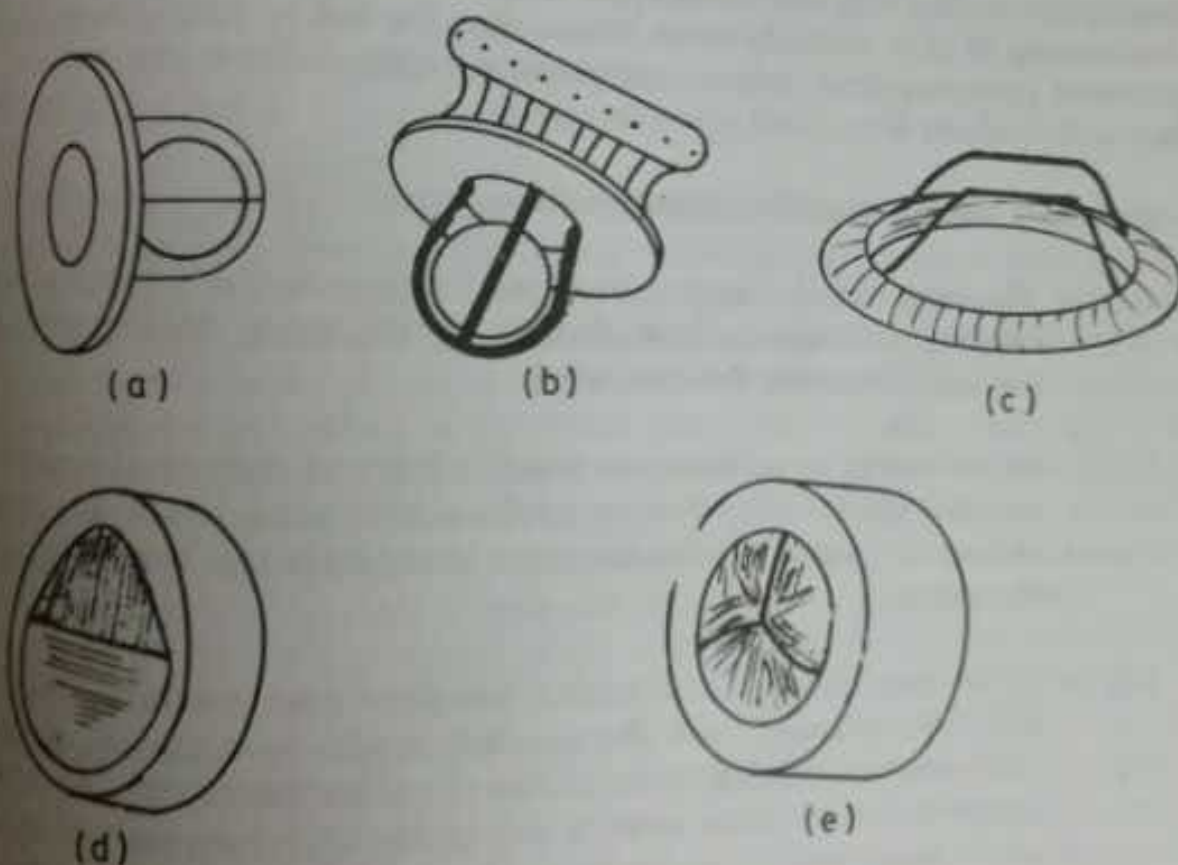


Fig.5.14. Different types of artificial heart valves

- a) Starr - Edwards mitral valve
- b) Magovern - Cromie aortic valve
- c) Kay-Shiley m'tral disc valve
- d) Gott butterfly mitral valve
- e) Leaflet valve

### 5.4.3 Different types of artificial heart valves

Most of the artificial heart valves are check valves of the caged-ball (Scandinavian type) or caged-disc (Alaskan type) variety. The ball or disc is made from silicone rubber to the natural seat from which the pathologic valve is removed. Starr and Edwards aortic valve has large orifice and small regurgitation. Starr and Edwards mitral valve (Figure 5.14(a)) differs from others such that there is a series of needle like projections which are screwed out during the installation procedure. These attach themselves to the ring of the valve to the tissue is eliminated and the operation can be performed in much less time. In the Kay Shiley mitral valve (Figure 5.14(c)) a caged disc replaces the silastic ball. This type is anatomically more suitable than other types. Gott butterfly mitral valve (Figure 5.14(d)) has quick opening and closing and large orifice. It has a disadvantage that it causes great regurgitation. Similarly the leaflet valve (Figure 5.14(e)) used as mitral valve has the same functioning of Gott butterfly valve. Now-a-days the ball or disc is made of various solid polymers (polypropylene, polyoxymethylene, polychlorotrifluoro ethylene, etc.), metals (titanium and vitallium alloys) and pyrolytic carbon.

### 5.4.4 Problems regarding artificial heart valves

- i) The early use of silicone rubber was found undesirable because of the swelling and dimensional changes of the valve. Further hemolysis and regurgitation were also produced.
- ii) In the aortic area, there are calcification and rupture of pericardial pouch within a few months when the artificial heart valve is used as a substitute for the aortic cusps. Calcification starts at the base and impairs the mobility of the valve.
- iii) In the Starr-Edwards aortic ball valve, there are some variations in the size of the ball after some months. Further this results in migration of the ball and embolization. The silicone rubber becomes susceptible to wear. During the implantation of valve, abnormality of implantation results a tight fit at the aortic root which alters the blood flow velocities. Similar variations have been observed in the Starr-Edwards mitral valve. In the mitral area, the most common problem with artificial valves has been the high incidence of thromboembolic (blocking of blood vessels) complications.
- iv) In some cases at the mitral site, the blood is slowly squeezing out and results clotting of blood. The blood clotting can even affect the operation.



the valve. The fabric coverings of both seat and cage show promise toward replacing the clot with tissue ingrowth.

- v) In some occasions, the ball itself has become deformed causing incompetency of the valve which decreases the normal operating efficiency. In few cases, the ball has actually escaped from its cage with tragic results.
- vi) There are some cases in which the blood leaks around the insertion site causing a small degree of insufficiency and clot formation.
- vii) Surrounding the insertion site there are mal formation and tissue growth which reduce the opening and closing actions of the valve.
- viii) Infection at the implantation site is usually fatal, although survivals have been reported after removal and replacement of the infected valve.

Despite these drawbacks thousands of people owe their lives to these artificial plastic replacements.

## DEFIBRILLATORS

A defibrillator is an electronic device that creates a sustained myocardial depolarisation of a patient's heart in order to stop ventricular fibrillation or atrial fibrillation. Ventricular fibrillation is a serious cardiac emergency resulting from asynchronous contraction of the heart muscles. This uncoordinated movement of ventricle walls of the heart may result from coronary occlusion, electric shock or abnormalities of body chemistry. Because of this irregular contraction of the muscle fibers, the ventricles simply quiver rather than pump the blood effectively. This results in a steep fall of cardiac output and can lead to death if adequate steps are not taken promptly. During fibrillation, the heart muscle fibers are continuously stimulated by adjacent cells so that there is no synchronised succession of events that follow the heart action. Ventricular fibrillation can be converted to a more regular rhythm by applying a high voltage shock to the heart. This sudden surge of voltage across the heart causes all muscle fibers to contract simultaneously. Possibly the fibers may then respond to normal physiological pacemaker pulses. The instrument for administering electric shock is called **defibrillator**. If the heart does not recover spontaneously after delivering the shock to the heart using a defibrillator, then a pacemaker may be employed to start the rhythmic contraction of the myocardium. The sudden cardiac arrest can be cured using a defibrillator and 80% of the patients will be cured from the cardiac arrest if treatment is given within one minute of the attack. An atrial fibrillation causes reduced cardiac output but is usually not fatal. It happens for the young people who are always nervous and can even be cured by drug therapy.